

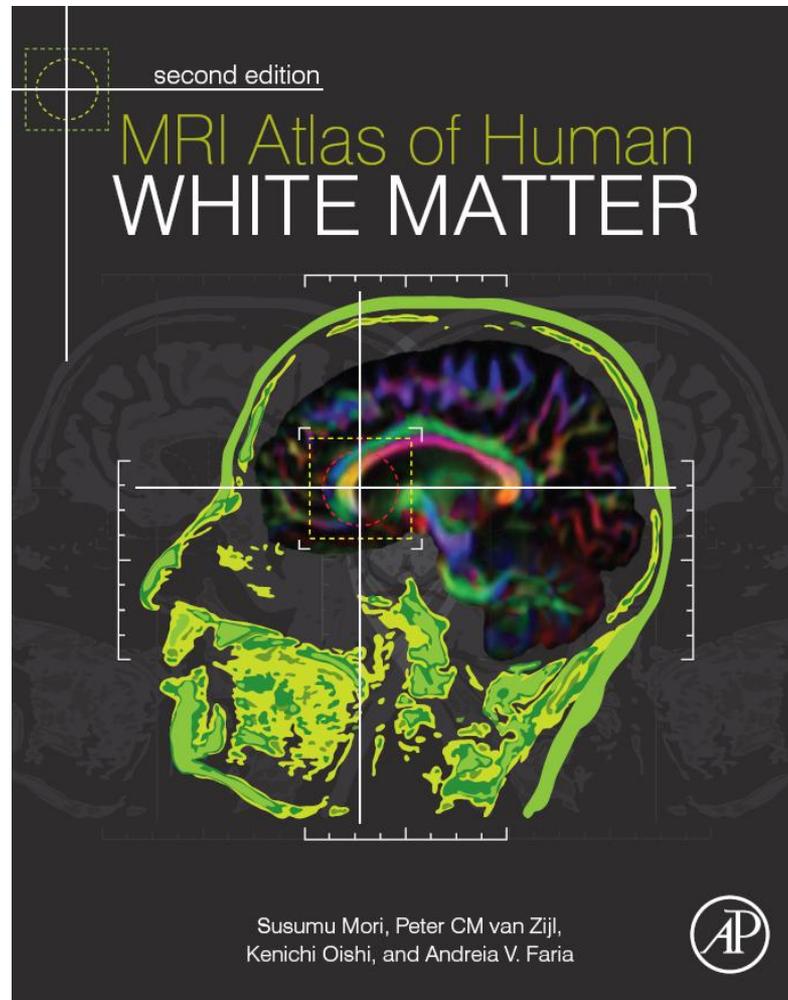
Diffeomorphic Shape Momentum, Computational Anatomy, & Neuroinformatics at 1mm Scale

Michael I. Miller



Toronto, June 2011

Neuroinformatics at 1mm Scale

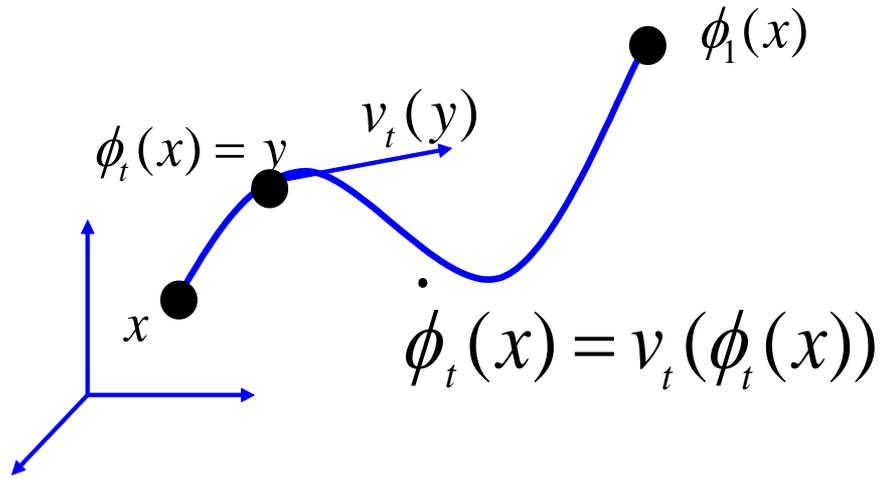
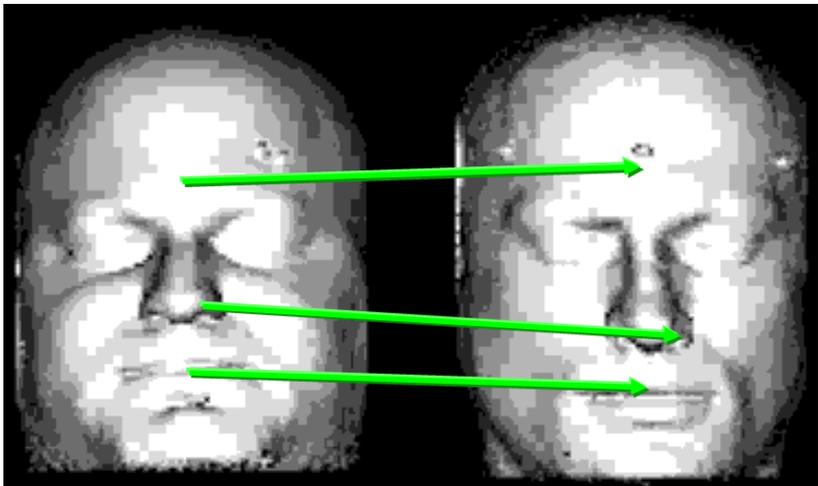


Computational Anatomy models human anatomy as an orbit of exemplars under the “diffeomorphism group”.

Populations are studied via templates with statistics encoded in template coordinates.

Diffeomorphic correspondences are used to carry the information from population coordinate systems to template coordinates.

We generate the diffeomorphism group as solutions of the ODE's.

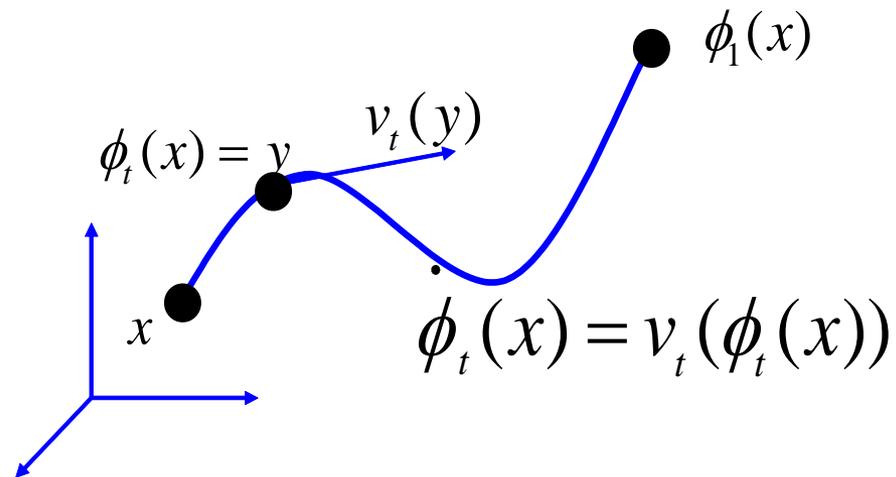
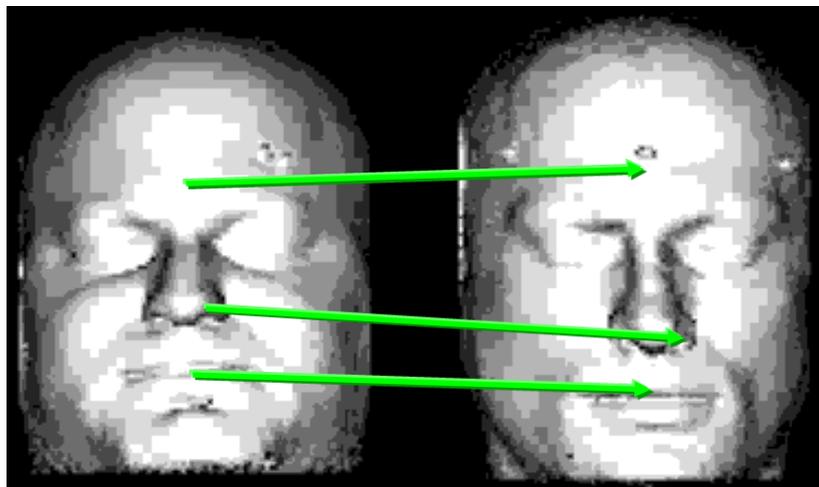


Lagrangian $\dot{\phi}_t(x) = v_t(\phi_t(x)), \phi_0 = id$

Eulerian $\dot{\phi}_t^{-1}(x) = -D\phi_t^{-1}(x)v_t(x), \phi_0^{-1} = id$
 D=Jacobian matrix $\begin{pmatrix} \frac{\delta v_i}{\delta x_j} \end{pmatrix}$

Deformable Templates Using Large Deformation Kinematics, IEEE. Trans. on Med. Imaging. Christense, Rabbitt, Miler, 1996.

We require the vector fields to be spatially smooth.



Variational Problem

$$\inf_{v \in V: \dot{\phi} = v(\phi)} \int_0^1 \underbrace{\|v_t\|_V^2}_{\int Av_t^* v_t} dt$$

smoothness
 $A = \Delta^{2p}, p \geq 1.5(\mathbb{R}^3)$

subject to
 $\phi_1 \cdot I \sim I'$
groupaction

Diffeomorphic Shape Momentum Conservation

$$\inf_{\substack{\dot{\phi}=v(\phi) \\ \phi_0=id, \phi_1=\varphi}} \int_0^1 \|v_t\|_V^2 dt = \int_0^1 \int_X A v_t^* v_t dt$$

Force Equation on Geodesics

$$\frac{d}{dt} M_t + (Dv_t)^* M_t + (DM_t)v_t + (\operatorname{div} v_t) M_t = 0$$

D=Jacobian
matrix $\begin{pmatrix} \delta v_i \\ \delta x_j \end{pmatrix}$

Momentum Conservation : $M = Av$

$$\frac{d}{dt} \int_X M_t^* D\phi_t w|_{\phi_t^{-1}} = 0$$

(interpret momentum as a function in action on smooth vector fields w)

$$M_t = |D\phi_t^{-1}| (D\phi_t^{-1})^* M_0 \circ \phi_t^{-1}$$

(as a vector function determined by initial condition)

One example: Steering the momentum via dense image matching.

$$\inf_{v \in V: \dot{\phi} = v(\phi)} \int_X \int_{M_t} A v_t^* v_t dt + \int_X |I' - \underbrace{I \circ \phi_1^{-1}}_{\phi \cdot I: \text{group action}}|^2 dx$$



Momentum Conservation Law

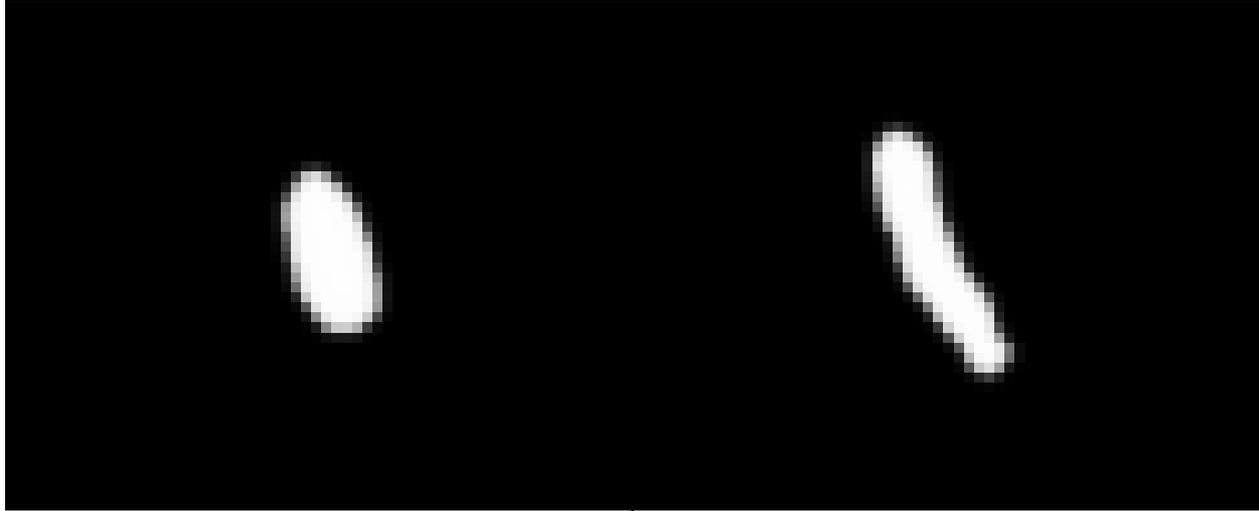
$$M_t = |D\phi_t^{-1}| (D\phi_t^{-1})^* M_0 \circ \phi_t^{-1}$$

$$M_t = \nabla(I \circ \phi_t^{-1}) |D\phi_{t,1}| (I' \circ \phi_{t,1} - I \circ \phi_t^{-1})$$

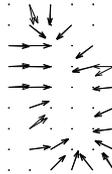
Normal to level lines of image.

smooth template
momentum
smooth

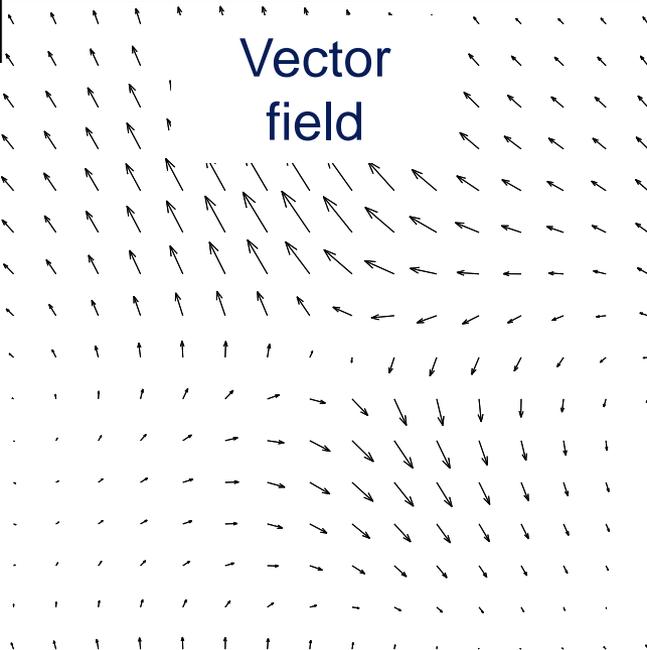
The momentum is a highly compressed representation of shape.



Momentum



Vector
field

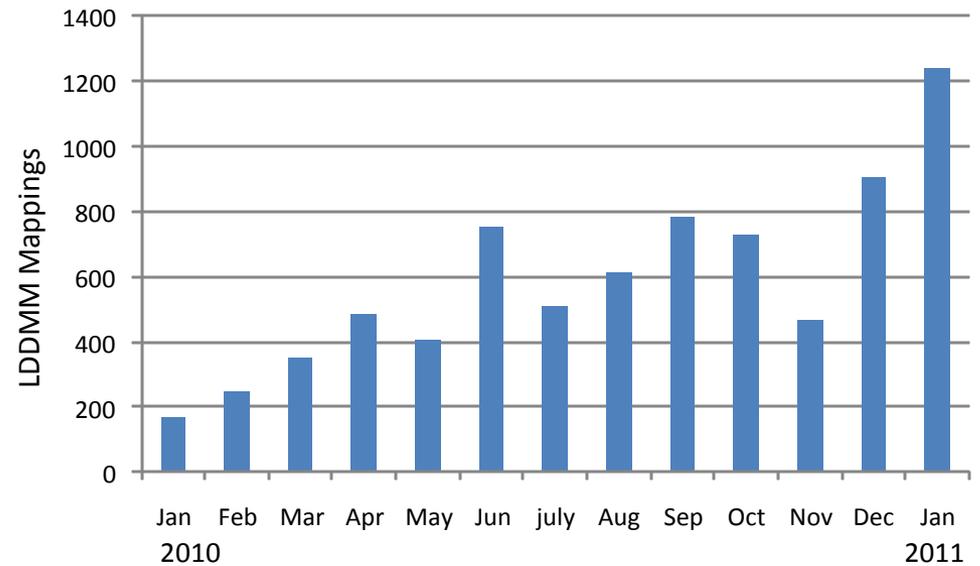
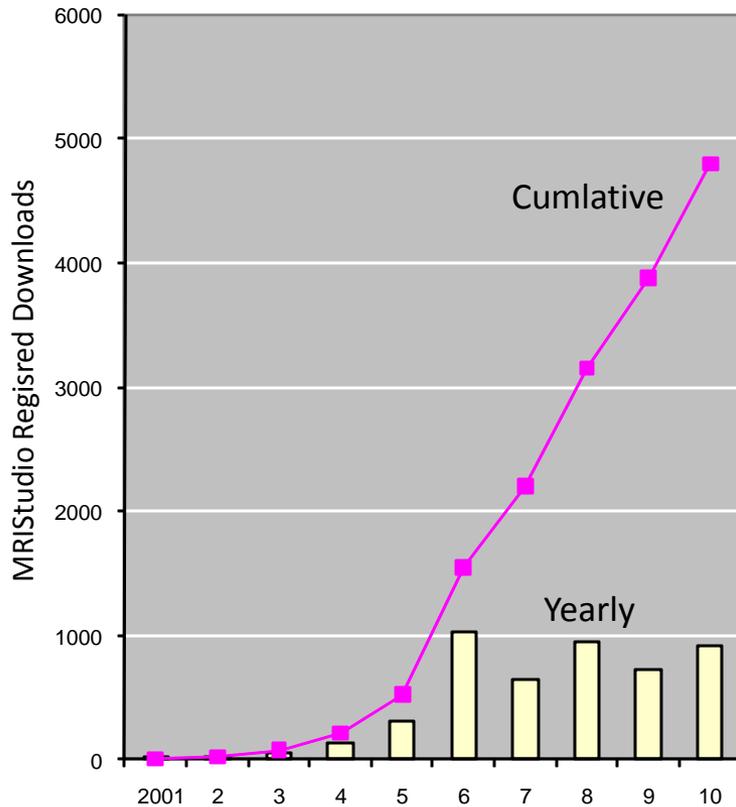


We have many methods of steering anatomical configurations one onto the other. We call these codes LDDMM.

- pointsets (landmarks, curves, surfaces)
- dense images
- vectors
- tensors

MRIStudio

<http://lists.mristudio.org/mailman/listinfo/mristudio-users>



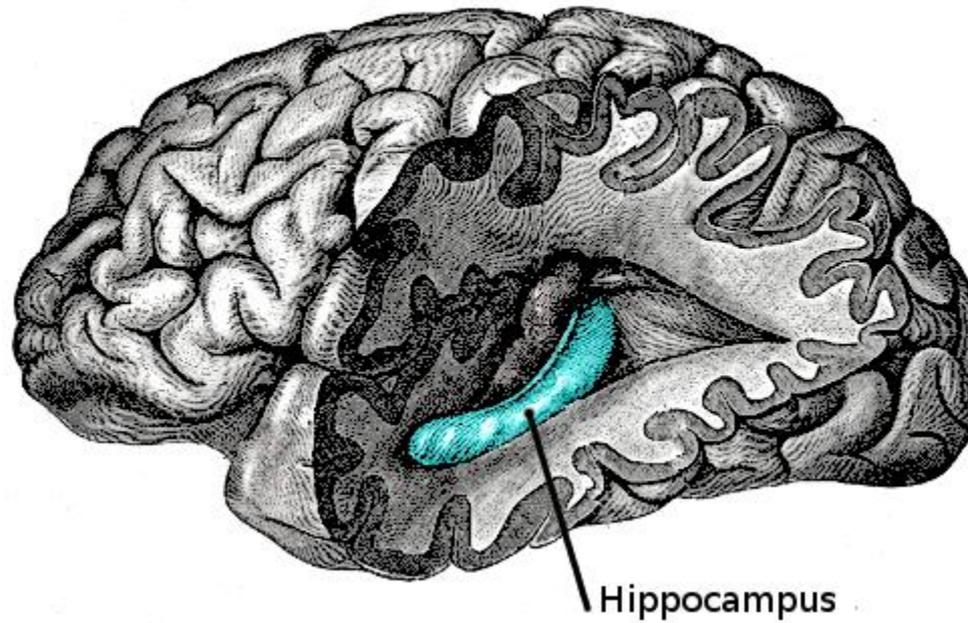
Computational Anatomy of Populations & Statistics on Shape Spaces

An Anatomical Model of Subcortical Human Anatomy

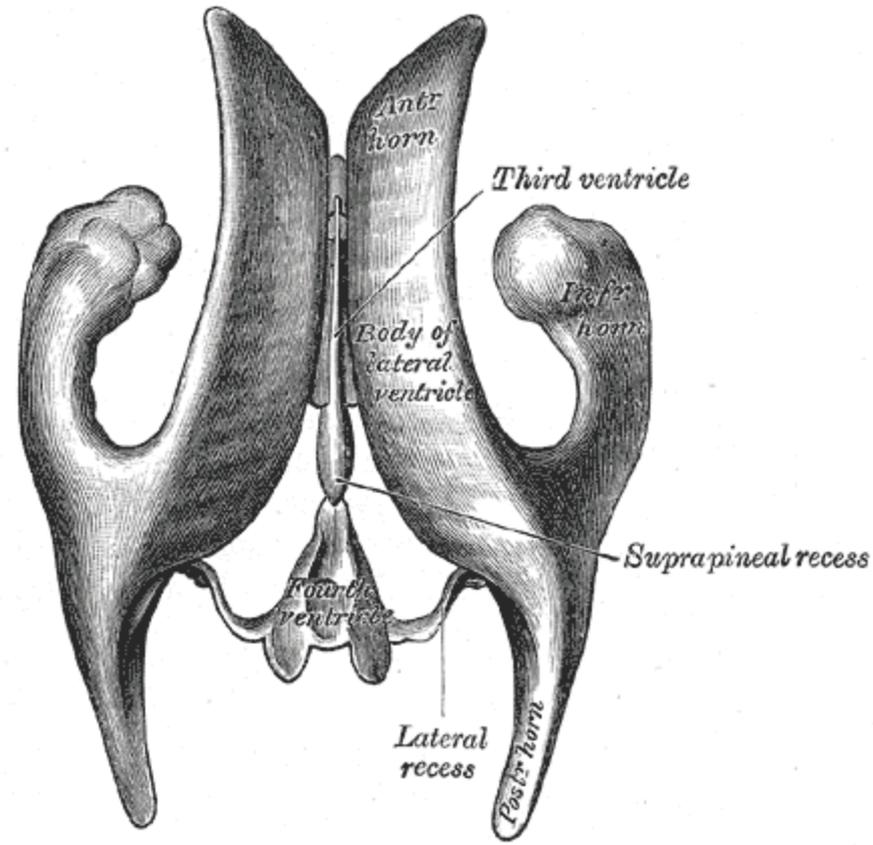
Daniel Tward

Anatomy at 1mm scale is clumpy.
Diffeomorphic Shape Momentum
provides a massive data reduction for
morphometry and helps with the curse
of dimensionality.

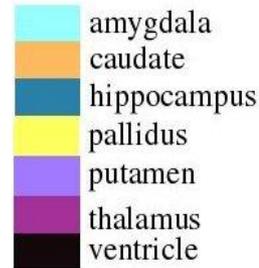
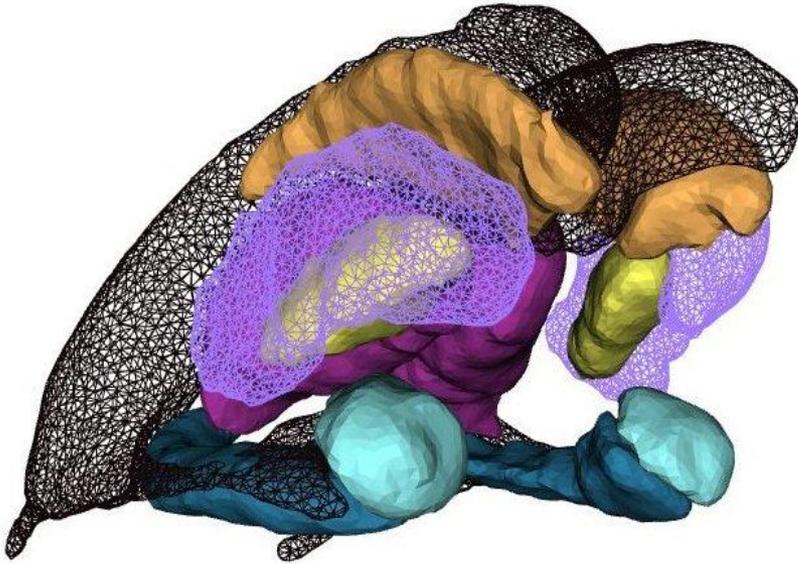
Subcortical Anatomy



Subcortical Anatomy



The Subcortical Random Field Model



$$M_0(dx) = \sum_{S \in R^3} \alpha(x) \sigma_S(dx)$$

$$V_0(\cdot) = \int_X \underbrace{K(\cdot, x)}_{3 \times 3 \text{ Green's matrix}} \underbrace{M_0(dx)}_{3 \times 1 \text{ Vector Measures}}$$

Dimensionality Reduction

$1/3 \times 3 \times 10E7 \rightarrow 7 \times 2 \times 10E3$

We use PCA and Surface Harmonics supported on anatomical structures for representing structure and function in curved anatomical coordinates

PCA requires training data.

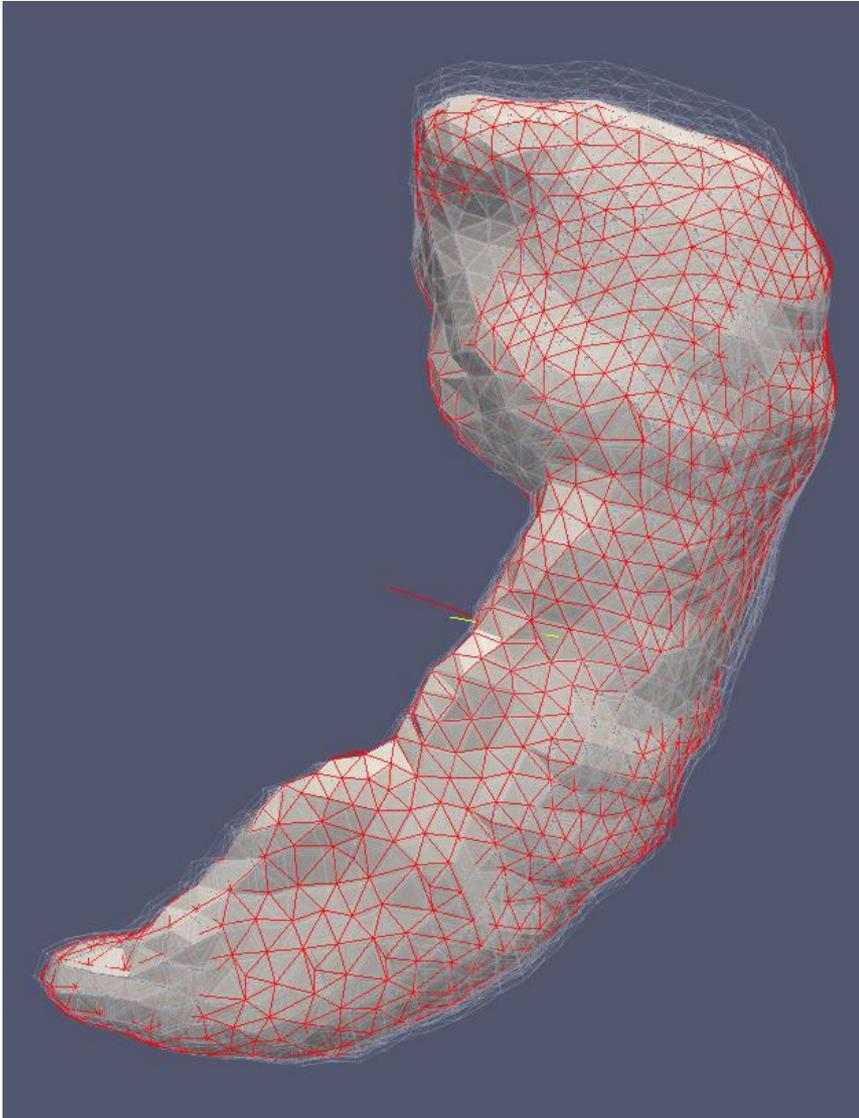
$$F = \sum_k F_k \phi_k$$

structure-function response-variables Laplace-Beltrami or PCA Basis

Representation of Subcortical Neuroanatomy in the Aging Population (Daniel Tward)

- A population of 600 whole brain anatomies which have been segmented (published) into all subcortical structures (ADNI, OASIS).
- A template atlas was generated from the population to which statistics on the Momentum is indexed.
- LDDMM surface mapping calculated the initial momentum carrying the template onto all 600 anatomies with 14 target surfaces.
- PCA analysis on the 600 momentum fields indexed over each of the surfaces taking into account the metric.

1 example: hippocampus template surface mapped to single target



- Surfaces mapped for all 600 left and right structures
- PCA was done on the momentum fields indexed to the template
- Shadow shows the amount of transformation from initial condition for one example.

Thank-You